



Novel Sensitive Electrochemical Immunosensor Development for the Selective Detection of HopQ *H.pylori* Bacteria Biomarker

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Introduction

- Helicobacter pylori (H. pylori)
- ✤ HopQ
- H. pylori utilizes its outer membrane HopQ proteins to facilitate the mechanism of trans fer of its pathogenic factor, such as CagA, to the host cells at early stages of *H. pylori* infection
- HopQ is considered an excellent biomarker for reliable, selective, and specific non-inva sive direct detection of *H. pylori* bacteria





Introduction biosensor platform

Immunosensors based on electrochemical methods

- Biomarker-based biosensors need to be one-time use (disposable),cost-affordable, simple, accurate, reproducible and sensitive
- Nanomaterials used in electrochemical biosensors: carbon-based nanomaterials, metallic nanomaterials
- Multi-walled CNTs (MWCNT)
- ✤ AuNP





Introduction

Screen-printed carbon electrodes (SPCEs)

Reference Working Electrode Electrode FDH Immobilization ✤ working electrode (WE) Counter Electrode via physical ✤ counter electrode (CE) adsorption Screen Printed Electrode ✤ reference electrode (RE) Apply BSA CV response Signal processing нсно Interaction between formaldehyde and FDH



Materials and Methods

Immunosensor Preparation

- Activation and Pretreatment of SPCE
- Nanocomposite Preparation and Surface Modification
- WE Preparation and HopQ-Ab Immobilization



Figure 1. HopQ biosensor interface development process schematic diagram.



Materials and Methods

Electrode Characterization, Analytical **Performance and Detection of HopQ**

- **Electrochemical Measurements** ×
- Surface Characterization by Scanning Electron Microscopy
- Detection of HopQ and Calibra * tion Curve
- Analytical Performance <u>cv</u>

otential

DPV

SWV



ш

OUTPUT



y=4.79+11.7x

Results

100 -

Current (µA)

Current (µA)

Electrochemical Measurements and Detection of HopQ

- ✤ Electrochemical Measurements
- ✤ Electrochemical Impedance **Studies**
- Immunosensor Analytical Performance

70 mV/s 60 mV/s 50 mV/s 50 40 mV/s 30 mV/s 20 mV/s Current (µA) 10 mV/s 0 0 -50 -50 Bare SPCE MES/Bare SPCE AUNP/MWCNT SPCE Ab/AuNP/MWCNT SPCE -100 BSA/Ab/AuNP/MWCNT SPCI -100 SPCE -0.4 -0.2 -0.6 0.0 0.2 0.4 0.6 0.8 1.0 -0.6 -0.4 -0.2 0.0 0.2 0.4 0.6 0.8 10 Potential (V) Potential (V) (A) (B) 110 SPCE 3000 · AuNP/CNT/SPCE 90 HopQ-Ab/AuNP/CNT/SPCE 70 BSA/HopQ-Ab/AuNP/CNT/SPCE 50 30 2000 10 Ina= 15.53 + 9.79X R2=0.998 -Z_{Im}/Ω L = -20.05 + -9.10X R²=0.992 -10 -30 -50 1000 -70 -90 -110 2000 3000 1000 4000 Z_{Re}/Ω 5000 6000 7000 800 10 (Scan rate)1/2 (mV/s)1/2 (D) (C) 8

100 mV/s

90 mV/s

80 mV/s

100



$$LOD = 10^{3.3 \times \partial} \alpha$$

$$LOQ = 10^{10 \times \partial}_{\alpha}$$



Figure 4. (**A**) SWV responses of BSA/HopQ-Ab/AuNP/MWCNT SPCE electrode with different HopQ concentrations, (**B**) variation in SWV peak current with respect to a blank solution vs. [HopQ] (and vs. Log[HopQ] for the inner plot). Error is the relative standard deviation for n = 3.

LOD = 2.0 pg/mL LOQ = 8.6 pg/mL



Results Comparison with other methods

Table 2. Limit of detection, detection range, and stability properties for different studies [61-65].

Ref.	Performance of Reported H. pylori Sensors							
	Interface	Detection Method	Biomarker	LOD (ng/mL)	Linear Range (ng/mL)	Stability at 4 °C (Weeks)		
[64]	CagA-Ab/ZnO*-T/SP-AuE	DPV	CagA	0.2	0.2-50	8–9	Up to 90%	
[62]	CagA-Ab/TiO ₂ -NPs/c- MWNCT/Pin5COOH/AuE	SWV	CagA	0.1	0.1-8.0	~3	90%	
						~6	50%	
[61]	CagA- Ab/Pt _{nano} /PEDOT/rGO/AuE	EIS	CagA	0.1	0.1–30	~8	60–70%	
[65]	BabA- Ab/Pd _{nano} /rGO/PEDOT/AuE	EIS	BabA	0.2	0.2–20	8–9	70%	
[63]	VacA-Ab/g-C ₃ N ₄ /ZnO/AuE	DPV	VacA	0.1	0.1-12.8	~2	94%	
This work	BSA/HopQ- Ab/AuNP/CNT/SPCE	SWV	HopQ	0.002	<mark>0.01–100</mark> -	4	~85%	
						8	~60%	

ZnO*-T: Irradiated Zinc Oxide Tetrapods, SP-AuE: screen printed gold electrode, AuE: gold electrode, TiO₂-NPs: Titanium oxide nanoparticles, c-MWCNT: carboxylated multi-walled carbon nanotubes, Pin5COOH: polyindole carboxylic acid, Pd/Pt_{nano}: palladium/platinum nanoparticles, PEDOT: poly(3,4-ethylenedioxythiophene), rGO: reduced graphene oxide, g-C₃N₄: graphitic carbon nitride.



Accuracy and specificity

Table 1

Comparison of Analytical Parameters of Different Detection Methods with the Presented Immunosensor

H. pylori detection methods	accuracy	specificity	time consumption
histopathology	95.3%	77.8%	about 7 days
PCR	94.5%		24 h
serology	86%	60%	more than 3 h
stool antigen test	80.2%	86.7%	1–4 days
rapid urease test	73.6%	85%	40 min
presented immunosensor	96.2%	87.03%	10–15 min



Selectivity and Cross-Reactivity



Figure 5. (**A**) Interferent study of BSA/HopQ-Ab/AuNP/MWCNT SPCE electrode with 5 ng/mL interferent concentration. (**B**) Interferent study of BSA/HopQ-Ab/AuNP/MWCNT SPCE electrode with 5 ng/mL HopQ antigen. (**C**) SWV peak current response of identically fabricated electrodes with the same criteria; the error bar is for n = 5.

Selectivity

✤ Cross-Reactivity



350

300

250

Current (µA)

100

50

0

- ✤ Reproducibility
- Shelf-Life Studies and Comparison with Other Platforms



Figure 5. (**A**) Interferent study of BSA/HopQ-Ab/AuNP/MWCNT SPCE electrode with 5 ng/mL interferant concentration. (**B**) Interferent study of BSA/HopQ-Ab/AuNP/MWCNT SPCE electrode with 5 ng/mL HopQ antigen. (**C**) SWV peak current response of identically fabricated electrodes with the same criteria; the error bar is for n = 5.



advantages and disadvantages



- ✤ highly enhanced sensitivity
- ✤ excellent selectivity
- lower detection limits
- Detection Ranges
- ✤ shelf-life
- ✤ simplified sample preparation
- ✤ cost affordability





Other studies

Methodology of Selecting the Optimal Receptor to Create an Electrochemical Immunosensor for Equine Arteritis Virus Protein Detection





Other studies

Novel Impedimetric Immunosensor for Detection of Pathogenic Bacteria *Streptococcus pyogenes* in Human Saliva





Conclusions

Why should we use immunosensors?









References

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Thank you for your attention